

Seppo Santavirta

1945–2005

Tissue Engineering and Biomaterial
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In memoriam

SEPPO SANTAVIRTA 5.12.1945–22.6.2005



Ortopedian ja traumatologian professori Seppo Sakari Santavirta menehtyi äkilliseen sairauskohtaukseen 59-vuotiaana 22.6.2005. Hän syntyi lääkäriperheeseen, mutta menetti molemmat vanhempansa jo kouluiässä. Siksi Seppo lähtikin suorittamaan asevelvollisuuttaan jo 17-vuotiaana ja nimitettiin aikoinaan Suomen nuorimmaksi vänrikiksi 18-vuotiaana. Tämä tinkimättömyys ja tavoitteellisuus leimasi jatkossakin hänen ammatillisia, urheilullisia ja kulttuurille pyrkimyksiään.

Asevelvollisuutensa suoritettuaan hän seurasi isänsä jalanjälkiä ja lähti Zürichin yliopistoon, josta hän valmistui 1972 lääkäriksi ja jossa hän suoritti ensimmäisen tohtorin tutkintonsa 1973. Palattuaan Suomeen hän teki Hyksissä kirurgiaan erikoistumisen ohella toisen väitöskirjansa väitellen 1979 Helsingin yliopistosta ja valmistuen samana vuonna kirurgian ja seuraavana vuonna ortopedian ja traumatologian erikoislääkäriksi. Hän oli pitkään Hyksin palveluksessa, mutta sai arvokasta koulutusta toimiessaan 1986–1996 Invalidisäätiön sairaala ORTONissa, jonka itsenäisyydestä noussutta laatutyötä hän aina arvosti ja jonka säilyttämisen hän näki tärkeänä. Seppo Santavirta nimitettiin Helsingin yliopiston ortopedian ja traumatologian professoriksi 1996 kaikkien asiantuntijoiden asetettua hänet avoimessa kilvassa ensimmäiselle sijalle.

Seppo perusti allekirjoittaneen kollegansa kanssa kansainvälisen monitieteellisen TULES-tutkimusryhmän, joka saavutti myös Suomen Akatemian huippuyksikön ja opetusministerin tohtorikoulun aseman. Monitieteellisen yhteistyön polttopisteessä ovat biomateriaalit ja niiden käyttö tekonivelkirurgiassa, ihmisen varaosina ja kudosteknologisissa sovelluksissa. Merkittäviin tutkimussavutuksiin kuuluvat timanttipinnoitteiden kehittäminen ja biomateriaalien kudosyhteensopivuuden selvittäminen. In nuce, todettiin että ihan oikeasti, "Diamonds are girl's best friend". Tästä tutkimusalueesta Seppo Santavirta teki kolmannen väitöskirjansa väitellen filosofian tohtoriksi biomateriaaliteknologian ja fyysikan professorin Reijo Lappalaisen ohjauksessa Kuopion yliopistosta vuonna 2003. Tämä oli Sepolle oikea nuorennuskuuri,

kun hän intoa puhkuen palasi nuoruuden voimien lähteelle sinne, mistä se hänelle parhaiten pulppusi: luovasta ja kovasta tieteellisestä työstä ja rehellisestä kilvoittelusta.

TULES-ryhmän avoimet ovet ja hyvä henki houkutteli yli 50 tutkijaa 21 eri maasta ryhmään tieteen viljelyyn, Sepon auran vaikutuspiiriin. Monet ryhmästä väitelleet ovat edenneet professoreiksi, dosenteiksi tai toimineet post-doceina ulkomailla. Kaiken kaikkiaan laajat kansainväliset yhteydet olivat ominaisia Seppo Santavirran työlle. Hän kuului useisiin toimituskuntiin kansainvälisissä ortopedisissa kliinisissä ja tieteellisissä sarjoissa. Seppo Santavirran ystävät, kirjaimellisesti ympäri maailmaa, ovat julkaisseet hänestä yksityiskohtaisemman nekrologin Acta Orthopaedica -lehdessä.

Seppo Santavirta piti luovan tutkimustyön lisäksi myös kliinisestä potilastyöstä. Huolimatta kirurgisesta spesialiteetistaan Seppo Santavirta muisti ja korosti aina potilaan integriteettiä ja oikeuksia, muistuttaen toimenpidevaltaisen spesialiteetin tunnustettuna mestarina toimenpiteisiin fiksioituneita lääketieteen kandidaattikisille siitä, että potilas on ihminen ja myös sellaisena kohdattava ja kohdeltava, kaiken tutkimuksen ja hoidon keskushahmona. Valtaenemistö opiskelijoista arvostikin suuresti riviopettajasta poikkeavaa elämäntaiteilijaa ja professoria, jonka opetuksessa innostuksen ja kiinnostuksen herättäminen aina ohitti passiivisen tiedon syötön. Seppo Santavirta tekiikin syvälle luotaavaa tutkimustyötä copingista ja potilaiden elämänlaadusta vaimonsa, vs. professori Nina Santavirran ja matemaatikko, FT Svetlana A. Solovievan kanssa.

Henkilönä Seppo oli lahjakas ja monipuolinen. Tämä heijastui hänen vapaa-ajan harrastuksissaan. Hän oli innokas urheilija.

Yleensä suomalaismies harjoittelee jopa yltiöpäisesti nuoruudessaan urheilun sitten jäädessä varhaisessa keski-ikässä. Seppo jatkoi urheiluharrastustaan koko ikänsä, treenaten elämänsä aikana lähes joka päivä. Oman pikaluistelijan aktiiviuransa jälkeen hän toimi Suomen Luisteluliitto ry:n puheenjohtajana 1978–1979 ja vuodesta 2001 alkaen Suomen Pyöräilyunioni ry:n ratapyöräilyjaoksen puheenjohtajana. Erinomaisen kuntonsa ansioista Seppo voitti suomenmestaruuskisoissa pyöräilymitaleita Masters-sarjassa, jollaiseksi sarjan nimi oli Sepon aloitteesta ja positiivisesti asioita tarkastelevan luonteen mukaan muutettu aiemman ikämiessarjan sijaan. Urheilijana Seppoa voidaan kuvata parhaiten sanoilla "vahva ja nopea". Toisaalta hän oli kiinnostunut taiteen harrastaja ja hankki merkittävää asiantuntemusta suomalaisesta taiteesta. Hän oli särmikäs oman tiensä kulkija, joka poikkesi tavanomaisesta parempaan. Parhaiten hän rentoutui kesäpäikällään Högsärassa perheensä parissa.

Sepon ennenaikainen menehtyminen on iso menetys suomalaiselle ortopediyhteisölle. Seppoa jäävät kaipaamaan ystävät ja varsinkin hänen rinnallaan uskollisesti koko elämän ajan taivaltanut vaimo Nina ja heidän rakkaat poikansa Torsten ja Robin.

Omnia conando docilis sollertia vincit (tutkimusryhmämme motto).

Yrjö T. Kontinen

Seppo Santavirta

1945-2005

Picture

1998, Photograph: Eero Roine

Seppo Sakari Santavirta, Professor of Orthopedics and Traumatology at the University of Helsinki, died after a sudden heart attack on June 22, 2005 at the age of 59. He was born into a physician's family but lost both of his parents when he was still at school. After military service, he followed in his father's footsteps and left for Switzerland to study medicine at the University of Zürich, from which he graduated in 1972. His first doctoral thesis, "Hyperplastische Schleimhautveränderungen im Dünn- und Dickdarm bei Morbus Menetrier" came from the same University in 1973. After returning to Finland, he started his specialization in surgery at the Helsinki University Central Hospital and at the same time he prepared his second Ph.D. thesis "Tourniquet ischaemia", which he defended successfully in 1979. He became a specialist in Orthopedics and Traumatology in 1980. During most of his active time, he worked for the Helsinki University Central Hospital, but he always valued his education and work at the Invalid Foundation ORTON (from 1986 through 1996). He was nominated Professor of Orthopedics and Traumatology at the University of Helsinki in 1996, after all four international experts had placed him in first place.

Together with Yrjö T. Kontinen, Professor of Medicine, Seppo founded an international and cross-scientific musculoskeletal diseases and inflammation research group (TULES). This group

achieved National Center of Excellence status from the Academy of Finland, and national Ph.D. Graduate School status from the Ministry of Education. The focus of the multidisciplinary research has been biomaterials and their use in arthroplasty surgery, as spare parts for humans and in tissue-engineering applications. The most important research achievements have been diamond coating of joint prostheses and studies on biocompatibility of biomaterials. Based on this research, Seppo Santavirta prepared and successfully defended his third Ph.D. thesis, "Compatibility of the totally replaced hip. Reduction of wear by amorphous diamond coating", and became a Doctor of Philosophy from the University of Kuopio in 2003 under the supervision of Reijo Lappalainen, Professor of Biomaterials Technology. Within the TULES group, Seppo hosted 50 researchers from 20 countries and many students of the group have advanced—becoming Professors, or working as postdoctoral fellows abroad.

Seppo Santavirta was a very flexible and creative scientist. As an athlete, he favored individual sports, but he was a good team worker, encouraging young people to make the most of their talents. He was also loyal to his senior co-workers, a man true to his word. His interest in sports led him to work with sports medicine and sports injuries, and later with traffic accidents and musculoskeletal diseases in general. Early on, he made substantial contributions to the understanding of occipito-atlanto-axial diseases. He described cervical spine involvement in trauma, in adult and juvenile rheumatoid arthri-

tis, spondylarthropathies, psoriasis and Down's syndrome, including the surgical treatment and outcome. This work often took him to Japan, where he had especially many good friends. Later, he started to work with biomaterials and joint replacements. Together with Kaj Tallroth, he observed a particularly aggressive form of aseptic loosening, which led to a beautiful series of publications on loosening of hip arthroplasties, covering pathobiological processes from foreign body reactions and immune responses to surgical treatment and long-term outcome. He recognized the role of foreign body reaction and delayed-type hypersensitivity early on, and sought co-operation with physicists working on plasma acceleration methods to produce high-quality diamond coating of artificial joint components with no wear and no corrosion. A strong link via a trusted friend, Doc. Mika Hukkanen, to the laboratory of Professor Julia M. Polak in London, led to several excellent publications on neuropeptides and innervation of the skeleton.

Seppo Santavirta liked research and clinical work equally and never forgot that patients are human beings, with feelings and lives of their own when away from the hospital bed, and he performed a great deal of coping and quality of life research together with his wife Docent Nina Santavirta and the mathematician Dr. Svetlana A. Solovieva, originally from Russia. Most of his research was characterized by strong international links and networking, and he was invited to the editorial boards of many international journals in his field. He devoted his most important work for scientific journals to *Acta Orthopaedica*, being a co-editor since 1989 until his death. During this time, he

edited hundreds of manuscripts and raised enthusiasm among many international researchers to write articles and reviews for *Acta*.

The untimely death of Seppo Santavirta ended a long orthopedics research career which showed no signs of waning; during his last year, Seppo published 15 scientific articles. Some of the last ones are published in this issue of *Acta Orthopaedica*: one Editorial on biotribology (page 613) and one review article on the medical treatment of rheumatoid arthritis, together with Yrjö T. Kontinen and coworkers (page 614).

Seppo was a talented all-rounder, which was reflected in his spare-time hobbies. He was an eager sportsman. After his active sports career in speed skating, he was the chairman of the Finnish Skating Association 1978–1979, and from 2001 he was chairman of the Track Racing Division of the Finnish Cycling Union. He was a connoisseur of the Arts, and attained considerable expertise in the Finnish Arts in particular. He had a charismatic personality, and would do things in his own way—preferring to take the better course rather than the regular and mediocre one. He relaxed and enjoyed life best with his family at their summer cottage on Högsåra Island in the Finnish Archipelago. His early death is a huge loss to the Finnish and international orthopedics community, to his friends and co-workers, and in particular to his wife Nina and sons Torsten and Robin.

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NOVEL DIAMOND-LIKE CARBON – POLYMER –HYBRID COATINGS PREPARED WITH THE FILTERED PULSED ARC DISCHARGE METHOD

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Introduction and aims: The development of the Diamond-like Carbon – polymer –hybrid (DLC-p-h) coatings is an example of the role of chance in materials development. In a failed DLC experiment, PDMS (polydimethylsiloxane) used as an electrical insulator was accidentally vaporised amidst the carbon plasma and a film of interesting properties was formed. The film could not be marked by any marker pens and neither stickers nor tapes could be attached to it. This led us to modify the FPAD system to produce similar coatings in a controlled manner. We introduced a specially constructed carbon-polymer cathode. By controlling the amount of the polymer component vaporised and sputtered by the carbon plasma (in effect controlling the pulse frequency of the system) coatings with a wide range of mechanical and wetting properties can be deposited. The method and the novel coatings are currently in the process of being patented.

Materials and methods: The FPAD unit is in a vacuum at a pressure of about 100 μ Pa. Carbon plasma arc similar to lightning is generated from the surface of the graphite cathode by discharging the ignition capacitor bank ($C=10-20$ pF). The plasma generated in the arc discharge then encounters a ring shaped graphite anode, which is at a higher potential ($U=500-6000$ V). As the plasma reaches the anode, the main capacitors are discharged. The main RCL-circuits parameters are typically the following: the tuning resistor $R\approx 0.1$ Ω , main capacitor capacitance $C\approx 10-30$ μ F, filtering solenoid inductance $L\approx 3$ μ H. The current (in the order of several kA) from the main capacitors is lead through a curved solenoid and a synchronized magnetic field (~ 1 T) is created to steer the plasma towards the sample and to filter out the unwanted neutrals and larger particles. The deposited DLC-p-h coatings combine the exceptional mechanical properties of the DLC coatings and the non-wetting properties of the “parent” polymer.

Table. Properties of PDMS and PTFE

Property	PDMS	PTFE
Density (g/cm ³)	1.1-1.6	2.17
Resistivity (Ω m)	10^{13}	10^{17}
Useful Temp. range/ $^{\circ}$ C	-115 to 315	-240 to 205
Chemical resistance	Good	Excellent

Contact and sliding angles. The property usually referred to when describing the non-stick properties of materials is the contact angle of distilled water droplet. Low surface energy materials show high contact angles and vice versa. However, the sliding behaviour can be measured directly by measuring the critical tilt angle at which the droplet starts to slide down an inclined plane called the sliding

angle of the droplet. It is important to notice that the contact angle and sliding angle are independent of each other. So, to evaluate how a surface truly repels liquids one has to study the behaviour of droplets on near horizontal planar tilt angles.

Results and conclusions: The Vickers hardness values of the DLC-PDMS-h coatings varied from 1 GPa to 70 GPa according to deposition speed [1]. The sp^3 fraction of 70% measured with ESCA corresponds well with the high hardness [1]. Higher deposition speed means higher amount of the polymer component and better hydrophobicity and lower hardness. It must be noted that the coatings are not isotropic as the DLC-polymer cathode heats up during the deposition process and the evaporation and sputtering of the polymer is enhanced towards the end of the deposition.

Both types of hybrid films showed high contact angles for water but DLC-PDMS-h coatings showed as a rule much lower sliding angles than DLC-PTFE-h. An oil drop slides easily down on DLC-PDMS-h coating and leaves no observable trace. However, because of the higher chemical resistance of PTFE the DLC-PTFE coating might be more suitable for some applications.

Extremely low sliding angle $0.15 \pm 0.03^{\circ}$ was measured on the surface of DLC-PDMS-h coating with a 20 ml distilled water droplet [2]. This is thus far the lowest sliding angle measured from a solid surface.



A carbon-polymer arc discharge. The ring shaped anode can be seen on the right, the sample is on the left.

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Research Scientist, Accelerator laboratory Department of Physical sciences, University of Helsinki; 1999-2004 (autumn). Research Scientist, Department of Medical Sciences, Biomedicum (autumn) 2004-. Alakoski is a member of the National Centre of Excellence studying biomaterials and a member of Biomaterial and Tissue Engineering Graduate School.

Ten selected representative publications or patents:

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EVOLUTION IN TRANSLATIONAL RESEARCH ON BIOMATERIALS: FROM REPAIR TO REGENERATION AND FROM BIOSTABLE TO BIOABSORBABLE MULTIFUNCTIONAL BIOMATERIALS

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Tissue engineering is a new concept to develop tissue grafts that can be used to treat lost tissues due to disease or trauma. To obtain successful tissue reconstruction, it is necessary to use proper biomaterial, cell-source and provide adequate vascularity. Thus, our work has focused on evaluating bioabsorbable materials both *in vitro* and *in vivo* and on developing vascularization models. First, we have continued translational research taking bioabsorbable tissue repair implants to the clinic. First stage comprised the use of both bioabsorbable and metal implants in CMF surgery. The second stage comprised all-absorbable system and in a third phase fine-tuning work focused on reducing the time of operation by using bioabsorbable tacks. Because of fibro-inflammatory tissue reactions induced by biodegradable implants, this was exploited to develop fibrous tissue joints to replace diseased joints in rheumatoid and osteoarthritic joints. A new animal model was developed. In other occasions, where inflammatory reaction was regarded as unwanted effect, anti-inflammatory releasing implants were developed and evaluated *in vitro* and *in vivo*. Because of osteolysis that may accompany the degradation of implants, bisphosphonate releasing implants were developed and being evaluated. To enhance the replacement of bioabsorbable devices with bone, osteoconductive element was added to the implants, e.g. screws and scaffolds that are evaluated *in vitro* and *in vivo*. To achieve proper graft or tissue engineered construct survival and functionality, vascularity is essential. Two models for microvascular tissue transfer were developed employing sheep and rabbits. Our studies have shown that it is possible to use bioabsorbable plates, screws and tacks to repair CMF bones. We have conducted an EU multicenter study on rare CMF syndromes and collected 165 cases [1]. Tacks were shown to reduce operation time which is important especially in infants. Adding bioactive glass as an osteoconductive component is being evaluated in animals and results are awaited. Preliminary results were encouraging [2] as showed even with genetically modified cells and cells derived from

syndromic (Crouzon) patients. Antibiotic releasing implants showed superiority to plain bioabsorbable and to titanium implants in significantly reducing bacterial attachment and biofilm formation [3]. Other multifunctional drug releasing implants have shown promise *in vitro*, and *in vivo* results are awaited. Tissue transfer models were successful [4] but cells may need to be combined with tissue flaps to enhance cartilage and bone formation. In conclusion, evolution of bioabsorbable implants has moved to the era of use of bioactive and multifunctional implants towards controlled tissue reactions and tailored clinical indications. Concepts of surgical therapy have also evolved from repair, to organ transplantation to arrive at reconstructive surgery employing tissue-engineered constructs.

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PRO-INFLAMMATORY CYTOKINE AND PROTEINASE CASCADES IN HOST RESPONSE AGAINST IMPLANTS

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INTRODUCTION

Periodontal diseases, particularly periodontitis is a chronic tissue destructive disease leading to loosening and loss of tooth in any age. Dental implants can be used to replace missing natural teeth with natural-looking and natural-feeling implants. Such implants, however, can loosen. Mechanisms responsible for periodontitis and peri-implantitis are somewhat similar. Loosening is thought to be due to mainly chronic infection with pocket bacteria/dental plaque-induced host inflammation and excessive/false directed mechanical loading.

We hypothesize that, cytokine induced neutrophil derived proteinases in gingival crevicular fluid and peri-implant sulcus fluid are important for the destruction of tissues surrounding both tooth and implant.

MATERIAL AND METHODS

Fluids and tissue samples were collected from five healthy controls (mean age 31) and seven patients with tissue destruction (mean age 46).

Immunohistochemistry was used for the localization of cytokine and proteases in tissue specimens. *Immunofluorometric assay* was used to analyze matrix metalloproteinase-8 or MMP-8 and MMP-9 levels in peri-implant sulcus fluid.

Western blots and *gelatin zymography* were used for the detection of pro and active forms of MMP-3,-8,-9. *Modified prourokinase substrate method* was used to assess MMP activities in cultured gingival fibroblasts stimulated with 10 ng/ml of tumour necrosis factor alpha.

RESULTS

Analysis of peri-implant sulcus fluid revealed that both MMP-8 and MMP-9 levels were high in patients who had loosening implants.

Western blots showed that gingival crevicular fluid from adult periodontitis contained

partially activated form of MMP-3. In healthy controls MMP-3 was found in latent or complexed form. Western blots also disclosed and zymography confirmed the presence of both latent and active forms of MMP-8 (or collagenase-2) and MMP-9 (or gelatinase B) in adult periodontitis. For MMP-8 and MMP-9 species both latent pro-MMP and active form were observed in periodontitis; whereas only its latent proform was found and only in low amounts in controls.

Matrix metalloproteinase activity in tumor necrosis factor- α stimulated and non-stimulated gingival fibroblasts revealed a significant increase of proform of MMP-3 but not in the active form of MMP-3.

CONCLUSION

Investigation of the levels of matrix metalloproteinases in peri-implant sulcus fluid and gingival crevicular fluid suggests that MMP-8 with MMP-9 may in part be responsible for the irreversible destruction of bone and soft tissues around implant and tooth. In addition to that the results suggest that fibroblast- and neutrophil-derived proteases cooperate to increase the matrix metalloproteinase burden in the gingival crevicular fluid of subjects with adult periodontitis or implantitis. Resident gingival fibroblasts produce proMMP-3 into gingival crevicular fluid, where it becomes activated, probably as a result of the action of the neutrophil-derived cathepsin G and elastase. Active MMP-3 then activates proMMP-8 and proMMP-9 leading to tissue degradation and loose of implants.

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EFFECT OF AMORPHOUS DIAMOND COATING ON SUBSIDENCE OF METALLIC PINS SIMULATING CEMENTED FEMORAL STEM IN CYCLIC FATIGUE TESTING

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INTRODUCTION

Bone cement is widely used for total hip replacement (THR). Its elasticity can distribute the point stresses between the bone and the stem. However, micromotion at the stem/bone cement interface and excessive subsidence of femoral stem cause wear particles and damage of bone cement which lead to periprosthetic osteolysis [1]. One of the theoretical benefits of titanium (Ti) alloy is a lower modulus of elasticity to reduce proximal stress shielding and bone resorption. However, Ti alloy is not recommended for cemented THR because Ti alloy stems may be severely damaged due to wear and crevice corrosion. However, advantages of bone cement and Ti alloy have a great potential for THR. Furthermore, reduction of excessive subsidence and micromotion is an important factor concerning to the longevity of the cemented femoral stem of THR. Amorphous diamond (AD) coating has turned out to be a promising biomaterial for artificial joint, due to excellent wear and corrosion resistance, biocompatibility, longevity and versatility [2,3]. Our hypothesis was that AD coating could improve stability at the stem/bone cement interface. The purpose of this study was to investigate the effect of AD coating on subsidence and micromotion of metallic pins in the model system for the cemented femoral stems.

METHODS

Widely used metallic biomaterials, Ti alloy, TiAl6V4 ($N=7$) and stainless steel (SS), AISI 316L ($N=12$) were used. The tapered pins (length 70 mm, angle 2.3°) had proximal and distal diameters of 10 and 8 mm, respectively. Different surface roughness values of the pins were achieved by grinding and polishing ($R_a = 50$ or 100 nm for Ti alloy pins and $R_a = 10$ or 100 nm for SS pins). Half of the SS pin set was coated with AD coating, 600-800 nm thick, by the filtered pulsed plasma arc discharge method [4]. The pins were cemented in nylon blocks (height 50 mm) with bone cement Refobacin®-Palacos® R (Biomet Europe, Dordrecht, The Netherlands). The minimum thickness of the cement mantle was 3 mm.

Cyclic fatigue testing (5 million cycles/pin) was carried out by using a servohydraulic tester (Instron, Canton, MA, USA). The vertical load profile was a scaled Paul's gait curve with a peak load of 0.850 kN at 10 Hz (ISO 14242-1). The torsional load with ± 3.750 Nm at 0.5 Hz (ISO 7206) was applied simultaneously. Testing was carried out in diluted bovine serum (total protein content 35 mg/ml). The vertical position was monitored throughout the tests by the software of the testing equipment.

RESULTS

The cumulative subsidence of the pins is shown in Figure 1A. Following tendencies of the subsidence were found:

with respect to coating: AD-coated < non AD-coated; with respect to surface roughness: rough < smooth; and with respect to material: Ti < SS.

The amplitude of vertical movement for a single loading cycle (micromotion at the interface) is shown in Figure 1B. For non AD-coated pins, the amplitude was high within 1,000 cycles and then reached a plateau, while the amplitude of AD-coated pins was more stable throughout the tests.

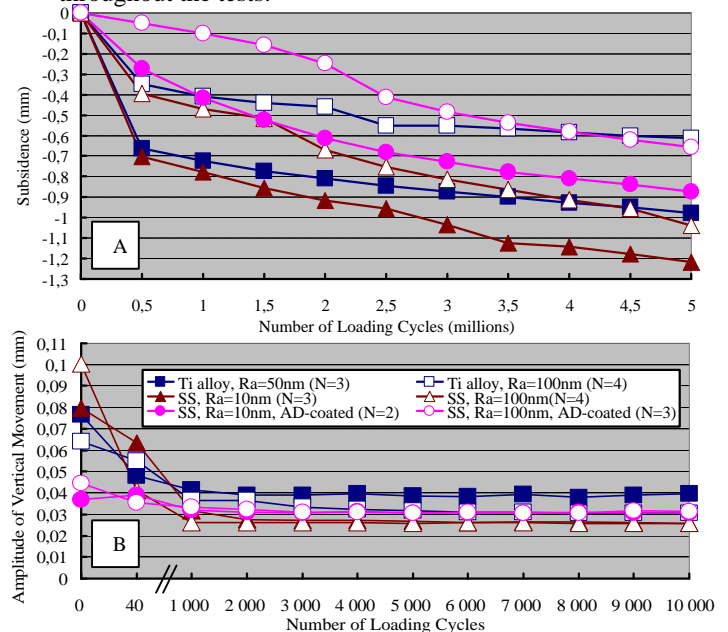


Fig. 1. Subsidence up to 5 millions (A) and the amplitude of vertical movement (micromotion) up to 10,000 cycles (B).

DISCUSSION AND CONCLUSION

Low subsidence of the AD-coated pins is most probably due to the surface characteristics of AD and higher stability of the interface for AD. Evidently, the rough pins are more stable due to difference in the shear forces at the interface. Lower subsidence of the Ti alloy pins is probably due to difference in the elastic modulus and the surface chemistry.

Based on the results of the micromotion within 1,000 cycles, debonding at the interface already occurred at the early stage in all specimens. Micromotion was least in the group of AD-coated SS pins. Thus, the interface is the most stable in this group. In conclusion, AD coating seems to be a potential material for surface treatment of femoral stem for clinical cemented fixation.

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BIODEGRADABLE TISSUE ENGINEERING AND INTERPOSITION ARTHROPLASTY SCAFFOLDS

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INTRODUCTION

Highly porous, three-dimensional biodegradable scaffolds with interconnective pores are essential for tissue engineering “living” implant to replace extracellular matrix for specific period of either cell culture or tissue healing or both. Several methods to manufacture scaffolds have been reported in the literature, for example solvent-casting followed by salt-leaching, freeze-drying and methods to prepare non-woven to 3-D structures. However, clear comparisons between the methods have not been published.

The aim of the studies has been to compare the important properties of the scaffolds manufactured by different methods from synthetic bioabsorbable polymers. An overview of the current situation of interposition arthroplasty project is given.

METHODS

In all cases poly-L-D-lactide 96/4 stereocopolymer is reported as a model polymer. Inherent viscosities varied from 1.8 to 5.5 dl/g and its influence to the scaffold properties was examined.

Five production methods were studied. As a standard, commonly used solvent-casting salt-leaching was performed using chloroform as a solvent. Melt-spinning hot-drawing followed by non-woven technique, braiding or knitting was the main interest in the studies. Also freeze-drying was experimented.

Several scaffold properties were followed, but in this presentation degree of porosity, interconnectivity of the pores and mechanical properties are reported from the scaffolds prepared. All the structures, including plain fibers, were tested *in vitro* (37C, pH 7.4, PBS).

RESULTS

Structurally the methods gave different scaffolds. Solvent-casting salt-leaching needed 90 wt-% of salt to obtain interconnective porosity for the scaffold and pores had shapes and dimensions of the salt particles. Textile techniques gave interconnectivity in all cases and pores had large range of sizes. Braided and knitted scaffolds had organized structure while others had randomly oriented pores.

Studied scaffolds had degrees of porosity from 40-50% (braided) to up to 90% (other methods).

Mechanical strength of the scaffolds was difficult to compare but relative strength retention *in vitro* described more the behavior. Solvent-cast salt-leached and non-woven scaffolds lost their mechanical strength completely in 20 weeks while others retained 50% of the initial strength for 24 weeks *in vitro*.

DISCUSSION

Manufacturing methods to produce scaffolds for tissue engineering can be chosen to meet the requirements of the application. Initial strength as well as strength retention either *in vitro* or *in vivo* can be tailored by changing the polymer used and also by using different production methods. Important advantages of textile technologies lie in their high throughput speed and large production capacity.

The knitted joint scaffolds are at the multicenter clinical studies for hand and feet small joints. These studies are giving awaited information of functionality of the first knitted scaffold structures used in humans.

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DIAMOND COATED SCREWS – VALIDATION OF TEST EQUIPMENT, EXPERIMENTS WITH HUMAN BONE AND MICROSCOPIC ANALYSIS OF MICROFRACTURES

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INTRODUCTION

Internal fracture fixation devices, such as screws, cause problems by failures during insertion and removal and by microfracture formation in bone tissue. Several factors including the surface finish of the screws affect the forces experienced by the screws. Smooth amorphous diamond (AD) coatings could prevent the problems related to the screws by low friction and inertness [1]. This study describes the methods and results for analyzing insertion properties of cortical bone screws and microfracture formation in cadaver human bone specimens.

METHODS

The equipment. Based on the ASTM standard F543-00 requirements a custom-made equipment for testing insertion torque was firstly manufactured and validated with homogenous test specimens [2].

Testing with human bone. Testing with cadaver human bone specimens was performed with stainless steel alloy screws [3]. Prior to testing, half of the screws was coated at the University of Kuopio with AD coating. Bone mineral density (BMD) of the test specimens was determined using a pQCT equipment. **Microscopic analysis.** Cylindrical bone blocks were prepared through dehydrating in ethanol and embedding into 2-hydroxyethylmethacrylate (HEMA). The blocks were then sectioned with a microsaw, ground and polished with a grinding system. Finally, the thin sections (about 25 µm) were stained with toluidine blue and examined with a photomicroscope using normal transmitted light [4].

RESULTS

The equipment. The results with low variation showed reliability of the equipment (see Table 1). The material and the rate of rotation had a clear effect on the torque values.

Testing with human bone. Both the BMD and the screw diameter had an effect on the torque values. AD coating reduced the torque needed for screw insertion up to 50%. Interestingly, the thinner screws needed relatively higher torque in the middle phase of the insertion than the thicker screws (Fig. 1).

Microscopic analysis. It was found that the AD-coated screws resulted in lower amount of fractures in the bone tissue, especially with the thinner screws (diameter 2.7 mm), see Fig 2.

Table 1. Maximum insertion torque in pine wood and Teflon. The screw diameter was 3.5 mm. Values are presented as the mean±SD (N=6). The range of values is also presented in the brackets.

Speed (1/min)	t_{wood} (Nm)	t_{Teflon} (Nm)
2.5	0.17 ± 0.03 (0.14–0.22)	0.13 ± 0.02 (0.10–0.15)
5	0.26 ± 0.05 (0.21–0.34)	0.18 ± 0.02 (0.16–0.21)
7.5	0.28 ± 0.04 (0.20–0.32)	0.17 ± 0.04 (0.11–0.22)
10	0.30 ± 0.05 (0.23–0.36)	0.20 ± 0.03 (0.14–0.23)

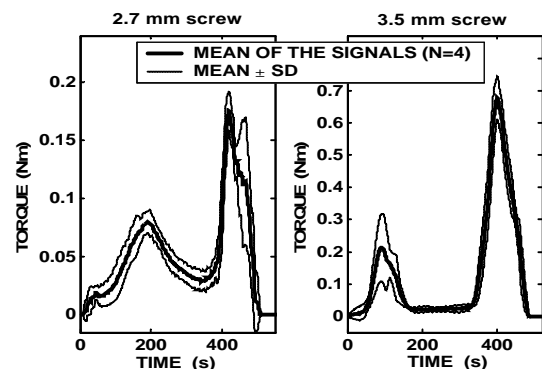


Fig. 1. Mean insertion torque indicated by the solid line and the range of the standard deviation by the dashed line (N = 4). Left; screw diameter 2.7 mm and right; screw diameter 3.5 mm. Note different scaling.

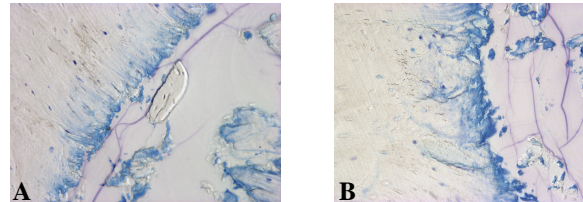


Fig. 2. Microscopic photographs of cortical bone after insertion and removal of bone screws (diameter 2.7 mm). A) Screw with the AD coating; B) Screw without the AD coating. Magnification 10x

DISCUSSION AND CONCLUSION

The custom-made equipment for testing of insertion properties of the screws proved repeatable results with low variation. Testing with human cadaver bone specimens showed that the insertion torque was significantly affected by the BMD and that the AD coatings provided reduced friction and torque. Thus, lower amount of energy is absorbed by the bone when using the AD-coated screws. Furthermore, microscopic analysis of stained thin sections is a useful tool for analysing microfractures in bone. In conclusion, AD coating seems to effectively reduce the damage formation, especially with thin screws.

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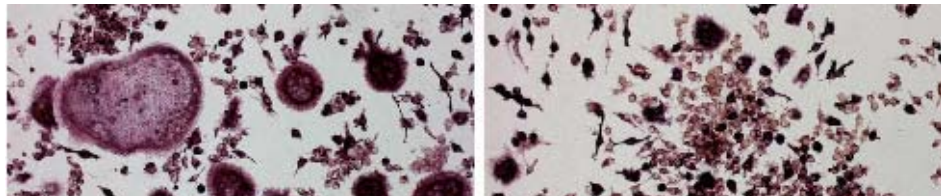
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FOREIGN BODY INFLAMMATION

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Control siRNA

The concept of “polyethylene disease” and then “particle disease” related to wear and material fatigue emerged concomitantly with the idea of aseptic loosening. Particle disease is considered to be caused by chronic foreign body inflammation. When the monocytes/ macrophages phagocytose very small particles of implant-derived synthetic materials and attempt to destroy them, the result is recruitment of more cells, local activation of phagocytes and resident cells, release of pro-inflammatory cytokines and formation of foreign body giant cells, osteoclasts and granulomas.

If the phagocytes sense danger, they take up a fight they can not win. The biological machinery, which can degrade and destroy all components of the extracellular matrix, including the tough collagen triple helix, is powerless in its fight against covalent and metallic bonds. The host defense system simply puts more effort into the process, leading to foreign body inflammation with all of its consequences. One inadvertent consequence is local production of tumor necrosis factor-alpha, interleukin-1 beta and, in particular, macrophage-colony stimulating factor and receptor activator of nuclear factor kappa B ligand. This stimulates osteoclast formation, shifting the delicate osteoclast-osteoblast balance in a negative direction so that linear and/or polycyclic aggressive granulomatosis arises. This is also an excellent model to study to study osteoclast biology.

The strategy for avoiding particle disease has been to minimize particle production through development of hard-to-hard bearings (ceramic-to-ceramic, metal-to-metal), the use of non-wearable surface coatings, such as diamond coating, and the use of highly cross-linked ultrahigh molecular weight polyethylene.



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29 already supervised PhD thesis works

50 past or present foreign visiting scientists from 21 different countries

Member in 10 Editorial Boards of International Peer Review Journals

Peer reviews for 52 journals

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CONVENTIONAL AMORPHOUS DIAMOND COATINGS

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INTRODUCTION

Most of the biomedical applications can be divided into two characteristic components: bulk material, which is mainly responsible for the mechanical and structural properties; and surface layer material, which interacts with the biological environment. The idea of surface modification or coating is to retain the desired bulk properties while modifying only the outermost surface. Because high quality amorphous diamond (AD) coatings deposited using ion or plasma beams are biocompatible, chemically inert, extremely hard and wear resistant, they are very potential to improve surface characteristics. However, biomedical applications are normally in very severe and demanding environment especially in long-term use. Therefore, the coating should last even a human lifetime without significant wear or delamination. This paper will show that this is a challenging task, but it is possible to achieve very good results, too.

METHODS

Experimental samples were made of commercial grade AISI316L, Ti6Al4V and CoCrMo alloys (Goodfellow, Cambridge, England) in the form of rods (8-10 mm in diameter), hip joint balls and cups or they were commercial bone screws. Before deposition of the AD coating, the rod samples were first mechanically ground with SiC paper (Mirka, Jepua, Finland) and polished progressively with diamond paste (Struers, Rodovre, Denmark) to give a typical surface roughness of (center line average) $R_a=10$ nm or 100 nm. Then, the samples were cleaned with acetone and ethanol using an ultrasonic washer. The vacuum chamber was pumped down to a vacuum of about 100 μ Pa and the samples were cleaned with an Ar⁺ sputtering ion gun. Proper intermediate layers were deposited on samples using a filtered pulsed plasma arc discharge unit or sputtering to improve adhesion between the substrate and AD films. By starting the AD deposition with high ion energy (140 eV) extremely strong adhesion was achieved. AD films were smooth (e.g., compared to coatings deposited with chemical vapor deposition methods) and the coatings were prepared at room temperature. The films were very pure; for example, the hydrogen content measured by the forward recoil spectroscopy method is < 0.1 at.% and the overall purity better than 99 at.% measured by the backscattering method. According to the measurements using the electron scattering for chemical analysis method, the relative amount of the sp³ diamond bonding in the films at the optimum deposition energy is around 80-85 %, which is a typical maximum value obtained with the plasma ion beams and with ion beams.

Relevant properties of AD coatings were studied using customized corrosion and wear tests and equipment as well as with simulators such as a commercial hip joint

simulator with six rotating stations and six soak-controls (ShoreWestern, Monrovia, CA, USA) or an Instron 8874 dynamic tester available at the University of Kuopio.

RESULTS

The main results of our extensive development and testing for AD coatings can be summarized as

1. AD-AD pair on articulating surfaces: an improvement in wear and corrosion resistance even by a factor of a million in long-term simulator testing [1,2]
2. AD-coated bone screws: reduction in friction and torque even by 50 %, less bone microfractures [3]
3. AD-coated metals against bone cement: major improvement in the stability and reduced wear and corrosion [4]
4. AD-coated Ti pins in a rat femur: significantly improved bone growth even compared to Ti [5]

DISCUSSION

In order to succeed in demanding environment of a human body, AD coatings must fulfill several requirements: high adhesion of the coating to the substrate, good corrosion resistance in biological fluids and high quality and surface finish. To achieve these goals, typically special procedures such as combination of different techniques, high deposition energies, intermediate layers or laminated structures are needed. Due to extreme properties of diamond, the coatings can improve corrosion and wear resistance even by a factor of million compared to conventional materials. This is a major advantage, e.g. in articulation surfaces of artificial joints, in bone screws or in other implant fixation systems with straight contact to living tissues or with bone cement. On the other hand, inertness and biocompatibility are important features in contact with body fluids like blood or saliva, e.g. in heart valves and teeth implants. Furthermore, surface properties of AD coatings can be optimized by proper dopants like Ca, P, F, metals, functional groups or monomers.

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Ten selected representative publications or patents during the last 10 years (total number of scientific publications including patents and extended abstracts about 150)

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ADAMs in the formation of foreign body giant cells and osteoclasts

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INTRODUCTION

The formation of multinucleated cells such as myotubes, macrophage-derived giant cells and osteoclasts is the result of cell-cell fusion of mononuclear precursors. The ADAMs (an acronym for A Disintegrin And Metalloproteinase) is a family of multifunctional proteins that exhibit a significant similarity with snake venom metalloproteases and are involved in cell-cell fusion processes [1]. As fusion molecules, ADAM12 and ADAM9 are involved in cell-cell fusion processes and participate in myoblast fusion and, also in osteoclast fusion.

METHODS

Immunohistochemical staining

Cryostat sections are fixed in acetone and incubated with ADAMs antibody.

Western Blot

SDS-PAGE was run. The gels were blotted onto nitrocellulose membrane. Then incubated with ADAMs antibody.

In Situ Hybridization

Sections were hybridized with Dig-labeled RNA probe.

Monocytes isolation and osteoclasts induction

Monocytes were isolated from buffy coat of healthy blood donors and cultured with M-CSF and RANKL.

Flow cytometry

Peripheral blood mononuclear cells were incubated ADAMs antibody and were analyzed by flow cytometry.

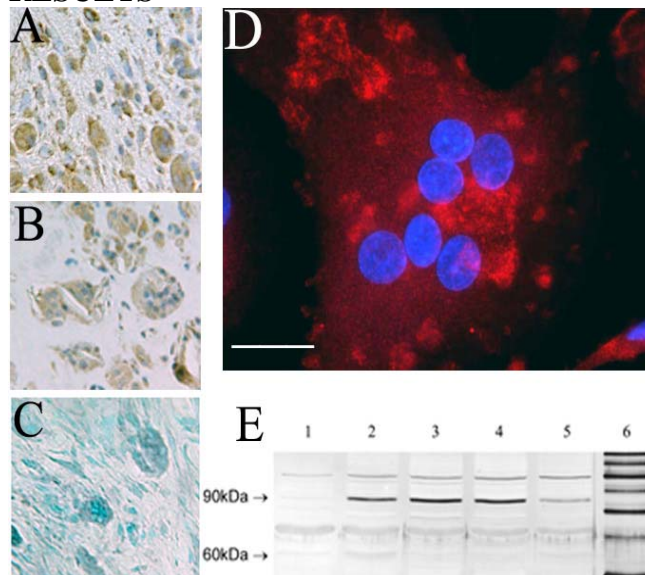
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RESULTS



Immunohistochemical staining of ADAM 12 in synovial membrane-like interface tissue from revision total hip replacement operation showing macrophage-like cells (A) and multinuclear foreign body giant cells (B) are ADAM 12 positive. In situ hybridization of ADAM 12 with antisense probe. ADAM 12 mRNA was detected in mono- and multinuclear cells (C). Immunofluorescence staining of M-CSF and RANKL stimulated human monocytes at culture day 14. ADAM 12 staining is shown together with nuclear counterstaining of the same field (D). ADAM 9 (E) Western blotting of human peripheral blood monocytes stimulated with M-CSF and RANKL for 1 day, 3 days, 7 days and 14 days (lane 1-4). Lane 5 demonstrates in non-conditioned medium and lane 6 demonstrates standards. A 60 kDa band is seen corresponding to fusion active form of ADAM 12.

DISCUSSION

Upon M-CSF and RANKL costimulation of human monocytes the proportion of ADAM 12 positive cells increased and they formed multinuclear giant cells and osteoclasts at day 14. In situ hybridisation disclosed ADAM 12 and ADAM 9 mRNA containing in mononuclear cells, often in a close spatial relationship with multinuclear cells present in interface tissue around loosening implants [2, 3]. In conclusion, ADAMs are involved in cell-cell fusions resulting in multinuclear giant cell formation.

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COLLAGENOLYTIC ENZYMES IN OSTEOBLASTS AND UNDIFFERENTIATED MESENCHYMAL CELLS DURING OSTEOGENIC DIFFERENTIATION

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OBJECTIVE

To study the presence and role of collagenolytic enzymes in bone forming cells in order to better understand the mechanisms of formation and maintenance of bone extracellular matrix.

DESIGN

Immunohistochemical stainings were performed for decalcified trabecular bone collected from patients operated due to the fracture of femoral neck. *In vitro* studies were performed using osteoblast-like cells and human bone marrow mesenchymal stem cells (MSCs) that were differentiated *in vitro* towards osteoblast phenotype with dexamethasone, ascorbic acid and β -glycerolphosphate.

RESULTS

Immunohistochemistry with antibodies against cathepsin K, the principal

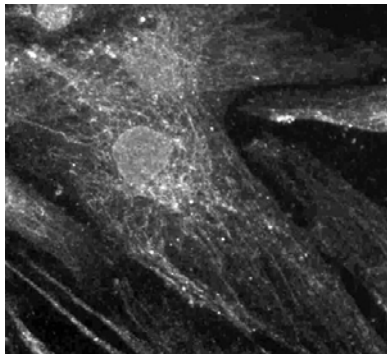


Fig. Immunostaining for cathepsin K in osteoblast-like cells.

collagenolytic proteinase in osteoclasts, showed cathepsin K immunoreactivity in bone lining cells, cuboidal osteoblasts and some osteocytes. Isolated osteoblast-like cells produced cathepsin K *in vitro* shown by the presence of both 42 kDa pro- and 27 kDa processed cathepsin K in cell culture medium. Quantitative RT-PCR showed relatively high cathepsin K mRNA production in isolated osteoblasts (382 ± 124 copies per one PBGD mRNA copy, in comparison to 5 ± 2 copies of MMP-13). Cathepsin K mRNA level was significantly reduced, when the cells were cultured under conditions of osteogenic differentiation (after 28 days 17 ± 7 cathepsin K mRNA copies per PBGD copy). Bone marrow derived hMSCs, after 28 day of osteogenic differentiation, showed similar levels of cathepsin K mRNA expression.

DISCUSSION

The cathepsin K expression by osteoblasts may contribute to organic bone matrix remodeling and recycling of improperly processed collagen I. The importance of osteoblastic cathepsin K to pathologies characterized by abnormal bone matrix turnover remains to be studied.

ACKNOWLEDGEMENTS

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EFFECT OF THIRD-BODY PARTICLES ON THE WEAR OF METAL-ON-METAL, CERAMIC-ON-CERAMIC AND DIAMOND-ON-DIAMOND THRs

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INTRODUCTION

Wear debris induced periprosthetic bone loss and aseptic loosening is regarded as the main long-term problem of prostheses and contributes to the reduced longevity of total hip replacements (THRs) [1-2]. Due to high hardness and durability ceramic-ceramic bearings in THRs have potential to provide an osteolysis free solution for hip arthroplasty.

Bone cement assists in distributing stresses between bone and metal stem. Unfortunately, micromotion at the interface between implant and bone may lead to the release of a large amount of bone cement particles [3-4]. In addition, stress concentrations at the implant/bone cement interface may lead to microfracture of bone cement. Metal, polymer, and bone cement debris can generate third body wear of the metal and polymer prosthesis components and finally lead to aseptic loosening [5-6]. Especially, bone cements contain typically about 10 wt.% ceramic (BaSO₄ or ZrO₂) particles as a X-ray contrast agent. There have been several studies on the wear of UHMWPE with third body particles in hip joint simulators, but no reports of similar systematic studies for hard sliding pairs: metal-on-metal (MOM) and ceramic-on-ceramic (COC). However, ceramic particles can severely damage metal surfaces and coatings.

The aim of this study was to compare the wear volumes and wear debris generated from MOM, COC and AD coating-on-AD coating hip replacements under third body wear conditions in the same hip joint simulator.

MATERIALS AND METHODS

Different types of THRs tested are illustrated in Fig. 1. They were all modular systems including a ball, a cup insert and a shell for non-cemented fixation. Amorphous diamond (AD) coating (20 microns thick) was deposited using a filtered pulsed plasma arc discharge technique.

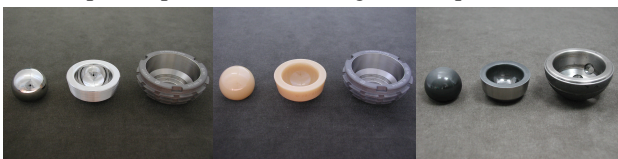


Fig.1. MOM (Zimmer Protasul-21WF), COC (Zimmer Cerasul), and AD-on-AD (custom made) test pairs.

Wear testing of modular implants was performed with a commercial hip joint simulator with six rotating and dynamically loaded stations and six soak-controls (ShoreWestern Manufacturing Inc., Monrovia, CA, USA). Cyclic loading of 5 million cycles corresponded to a Paul gait curve with a peak load of 3kN and a frequency of 1 Hz. Diluted bovine serum with standard additives of EDTA and antibacterial agents were used as a lubricant. The serum was filtered through a 0.2 micron filter and had a total protein content of 35 mg/ml after dilution. The first 1.5

million cycles was tested without third body particles. Bone cement particles (containing 10 wt.% ZrO₂) were added in concentration of 1mg/ml after 1.5 million cycles and 10 mg/ml after 2.5 million cycles. Then the last 1.5 million cycles were tested without third body particles. Volume weighted mean size of bone cement particles was 110 µm. The serum with/without bone cement particles was replaced every 500 000 cycles. The oscillatory cup motion was ±23° about a horizontal axis and a cup and a ball were mounted in anatomic position. Load and friction were monitored throughout the tests.

RESULTS

The wear of MOM pairs increased significantly when debris was added in the lubricant (Fig. 2). The wear of COC and AD-on-AD was below <0.2 mm³/million cycles. Overall wear of the MOM pairs was 13.5 mg after 5 million cycles.

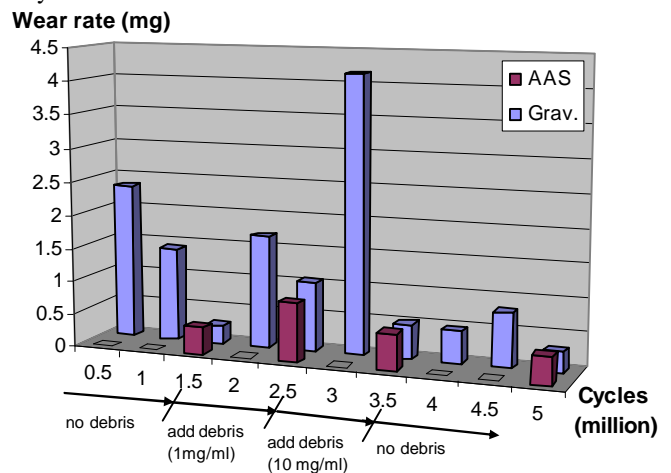


Fig. 2. Wear rate of MOM pairs determined by AAS or gravimetry.

DISCUSSION AND CONCLUSION

MOM: third body particles can significantly increase wear and release of ions. COC: wear rate is very low even with bone cement particles. Tolerances in fixation are critical and can lead to fracture. This study shows that AD coatings do not delaminate or wear even with ceramics particles when the coatings are thick enough to withstand high stresses in point contacts. Furthermore, they are effective against corrosion [7].

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Master's degree: 1998 Joensuu, Finland: Heterogenous hydrogenation of
d-xylonic acid, using ruthenium and rhodium-molybdenum catalyst

Doctorate: 2005 Kuopio (estimation)

Relevant work experience:

Assistant researcher, 1997-1998, 11 months, University of Joensuu; Assistant researcher, 1999-2000, 14 months, University of Helsinki; Researcher 2000-2001, 8 months, University of Kuopio; Project researcher 2001- University of Kuopio; Project researcher (Material testing and surface analysis) 2002- BioMater Centre; Project coordinator (Gas phase coatings) 2003- BioMater Centre.

Publications:

1. IC. Clarke, FW. Chan, A. Essner, V. Good, C. Kaddick, R. Lappalainen , M. Laurent, H. McKellop, W. McGarry, D. Schroeder, M. Selenius , M.C. Shen , M. Ueno, A. Wang, J. Yao, Multi-laboratory simulator studies on effects of serum proteins on PTFE cup wear, *Wear*, **250**(2001)188-198.
2. R. Lappalainen, M. Selenius, A. Anttila, Y.T. Konttinen, S. Santavirta, Hip simulator study of amorphous diamond – amorphous diamond THR couples, ESB 2002 conference (extended abstract).
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5. R. Lappalainen, M. Selenius, A. Anttila, Y.T. Konttinen, S. Santavirta, Reduction of wear in total hip replacement prostheses by amorphous diamond coatings. *J. Biomed. Mat. Res.*, **66B** (1)(2003)410-413.
6. H. Kuopanportti, E. Hotti, M. Selenius, R. Lappalainen, New environmentally friendly method to coat metal with wood distillate, ICECFOP Conf. Proc., Porto, Portugal, 2004, 1-7.
7. M. Selenius, S. Santavirta , R. Lappalainen , Simulation studies of the five most commonly used THR implants in Finland, 7th World Biomaterials Congress, Sydney 2004 (extended abstract).
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THE LONG-TERM EFFECT OF PLA BANDS (version II) ON THE HEALING OF STERNOTOMY IN THE SHEEP.

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Technion, Haifa, ISRAEL and Tampere Technical University, FINLAND

INTRODUCTION

The current project involves the clinical problems of management of bone healing. The patients undergoing open heart surgery often develop deep wound infection in the sternal bone. Today more older people than before (75 years), with all their potential medical complications, are undergoing cardiac surgery. There is a need for an *in-vivo* experimental model, that will be as close as possible to the clinical state in humans. Because of biomechanical reasons we have elected to use the sheep as our experimental model.

METHODS

On the bases of various tests, the sheep appears as an appropriate model for studies on bone healing. We have developed an *in vivo* procedure for standardization of surgically induced bone injury. Hence, we succeeded to check the effects of biodegradable PLA bands on the healing of sternotomy in sheep.

The surgical procedure : cutting the skin, exposing the sternal bone, cutting the sternal bone by using an electrical saw and thereafter, closure of sternotomy via biodegradable (fig 1) PLA bands (fig 2) following by closing the overlying tissues. Control sternotomies were closed using stainless steel wires (fig 3).

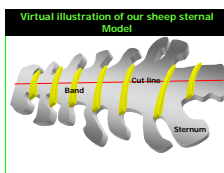


fig 1

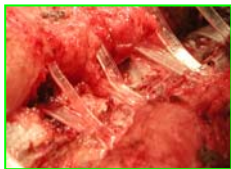
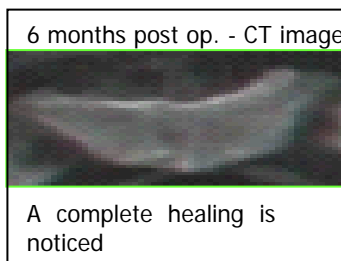
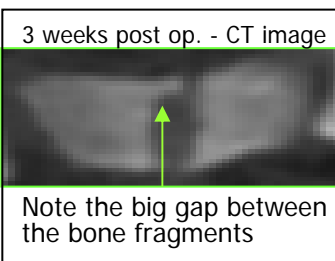


fig 2



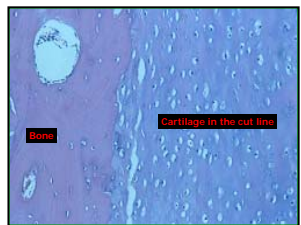
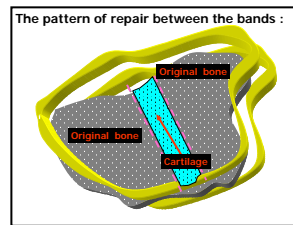
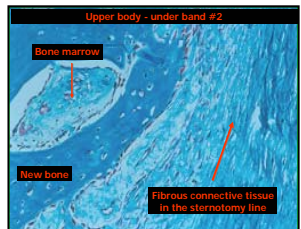
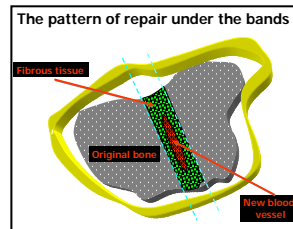
fig 3

RESULTS



REPAIR CHARACTERISTICS : 7 WEEKS POST - OP

	INTACT (CONTROL) #1141	7 BANDS #1072	8 WIRES #1115	LEMA & RIMA #1225
BMD (g/cm ³)	0.954	0.652	0.356	0.153
BONE-SCA (% disoste)	0.8125	0.8659	0.8332	0.817 (9 days)
COMPRESSION LOAD (N/mm)	177.6	212	68.3	65.3
BENDING MOMENT (Nmm/mm)	666	733	355	140.3



DISCUSSION

- Based upon our findings *in vivo* we can sum up:
1. By 6 months post op. the CT images revealed the restoration of the bone architecture to its original form.
 2. By 11 months post op. the microscopic findings indicated neovascularization, which facilitated the formation of new bone.
 3. From the clinical point of view, the bands in their present form enabled the healing of the bone throughout the osteotomy line.
 4. The bands are biocompatible (after 11 months *in vivo*).

RECOMMENDATIONS

1. Make the bands more flexible.
2. Self-locking bands will shorten the surgery.
3. Improve the quality of the needle & its attachment to the band.

ACKNOWLEDGEMENTS

Funded by the Institute of Biomaterials, Tampere Technical University, Tampere.

Professor Michael Silbermann

Professor Michael Silbermann (D.M.D.; Ph.D., and certified specialist in oral and maxillo-facial surgery) is head of the laboratory for musculoskeletal research and the Dr. Irving and Jeannette Benveniste Chair in Medicine at the Faculty of Medicine in the Technion – Israel Institute of Technology, Haifa, Israel. He has gained international reputation through multinational research projects related to bone and cartilage development, metabolism and senescence. These have been funded by Israel, U.S. and German research agencies (Israel National Council for Research and Development, Ministry of Science; Chief Scientist Office in the Ministries of Health and Commerce and Industry); NIH, USAID, and BSF in the United States; BMBF, GBF and GSF in Germany). Large financial support was obtained also from industries: Laser Industries, Israel; Teva Pharmaceutical Industry, Israel; General Biotechnologies, Israel; Diagnostic Technologies, USA; Nordisc Gentofte, Denmark; Surgical Biopolymer Materials, France; Medical Bracing Systems, Israel. He has recently been awarded a European Commission Grants #70786, 71329, and 71395. He has been awarded research fellowship grants by the American Association of Dental Research, The Fogarty Foundation (Bethesda, MD), EMBO, Max Planck Society, and Japan Society for the Promotion of Sciences.

He has undertaken a number of senior national and international administrative duties especially in the field of biomedical research:

- 1974-1994 Chairman of the Department of Anatomy and Cell Biology, Faculty of Medicine, Technion, Haifa, Israel
- 1989-1992 Vice Dean for Research and Development and Dean of the Faculty of Medicine, Technion, Haifa, Israel
- 1993-1996 Chief Scientist, Ministry of Health, Israel
- 1994-1997 Member and Chairman of the Board of Governors, the United States-Israel Binational Science Foundation
- 1995-1997 Member of the National Council for Research and Development, State of Israel
- 1995-1997 Member of the Committee for the Promotion of Infrastructure in Biomedical Research, Ministry of Science, Israel
- 1995-2001 Member of the Foulkes Foundation (United Kingdom) Committee for Doctoral Fellowships. The Israel Academy of Sciences and Humanities
- 1996-1997 Member of the National Steering Committee for FDA Regulations for GLP, State of Israel
- 1996-1997 Member of the National Committee for Ethics in Science and Intellectual Property, Israel
- 1996- Executive Director, the Middle East Cancer Consortium
- 1996-1997 Member, BIOMED2, Program Committee, DGXII, EC, Brussels, FP4
- 1997-2000 Member, Scientific Committee of Medicinal Products and Medical Devices, DGXXIV, EC, Brussels, FP5
- 1998-2000 Member, Risk Assessment Coordination Group, DGXXIV, Brussels, FP5
- 1998-2001 Chairman, National Committee for Examining Academic Specialty Training in Health, Social and Education Professionals, The Council for Higher Education, State of Israel
- 1999-2002 Evaluator, Directorate for Health Research, EC, Brussels, FP5
- 2000-2002 External Reviewer, Centers for Excellence in Biomaterials and Tissue Engineering, The Finnish Academy of Sciences, Helsinki
- 2002- Editorial Board European Journal of Cells & Materials
- 2002- Member, review Committee of Expression of Interest, EU, Brussels, FP6

Bibliography

251 original articles on *in vitro* systems of cartilage and bone, age-related changes in articular cartilages, osteoarthritis, and osteoporosis. In addition, research was conducted with respect to endocrinological involvement in the growth, development, and aging of skeletal tissues. Over 400 presentations in international and national scientific meetings. Organized 26 international workshops and conferences.

Tutoring

32 graduate students for MSc. and DSc degrees, 4 for MD degree, and 33 physicians (basic sciences as part of their specialty training).

FROM BASIC RESEARCH TO INNOVATIONS

Pertti Törmälä
TUT, Institute of Biomaterials
(on leave)
Bioretec Ltd., CSO

INTRODUCTION

This abstract comprises a short summary of surgical product innovations of bioabsorbable materials related to basic research of BRG-Center of Excellence between 2000-2005.

STUDIES OF BIOPOLYMERS

Melt extrusion of polymers and copolymers.

Solid state deformation-orientation.

Microstructure and properties of processed materials.

PRODUCTS MADE OF ORIENTED BIOPOLYMERS

Bioabsorbable screws, tacks and plates for fixation of craniomaxillofacial fractures and osteotomies (Bionx Implants Ltd.).

Autocompression fixation implants for orthopaedics and traumatology (Bioretec Ltd.).

Self-locking bands for closing of sternotomy after open heart surgery (Bioretec, Ltd.)

Instruments for installation of bioabsorbable fixation implants (KI-Technology, Ltd., EM-Technology, Ltd. and TH-Tools, Ltd.).

STUDIES OF BIOPOLYMER-CERAMIC COMPOSITES

Melt extrusion and molding of lactide copolymer-bioceramic (TCP or bioactive glass) composites:

- Structural studies
- Material technical properties
- *In vitro* and *in vivo* behaviour.

COMPOSITE PRODUCTS

Interference screws for fixation of ACL-transplants (Linvatec Biomaterials, Ltd.).
Osteoconductive fusion implants for vertebroplasty (Bioretec, Ltd.).

TISSUE ENGINEERING STUDIES

Regeneration of small joints with bioreplaceable joint prostheses.

PRODUCTS

Bioreplaceable small joint scaffolds (Linvatec Biomaterials, Ltd.).

DRUG-RELEASE STUDIES

Studies on antibiotic- and anti-inflammatory drug-releasing bioabsorbable polymers and composites.

PRODUCTS

Antibiotic releasing bone fracture fixation screws (Bioretec, Ltd.).

Osteoconductive, antibiotic releasing bone defect fillers (Bioretec, Ltd.).

FUTURE PRODUCT TRENDS

Bioactive and drug-releasing tissue management implants.

Reconstruction of damaged tissues with hybrid implants comprising bioabsorbable scaffolds and patients own cells (e.g. osteoblasts, fibrocytes, fat cells, chondrocytes or stem cells).



TAMPERE UNIVERSITY OF TECHNOLOGY
Institute of Biomaterials

**CURRICULUM VITAE
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PERTTI TÖRMÄLÄ
24.10.2005**

PROFESSIONAL PROFILE

Over 25 years of innovative, scientific and entrepreneurial experience in science and technology of bioabsorbable composite materials for surgical applications. Founded the first successful international company specializing in the development, production and marketing of bioabsorbable implants for management of musculoskeletal and cranio-maxillofacial traumas.

EDUCATION

University of Helsinki (Helsinki, Finland)
Ph.D. in Polymer Science, 1974

University of Helsinki (Helsinki, Finland)
B.S. Medicine, 1973

PROFESSIONAL AFFILIATIONS

Biomedical Engineering Society
EC Committee for Surgical Implants
European Society for Biomaterials
International Society for Artificial Organs
IUPAC Macromolecular Division Committee

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EMPLOYMENT HISTORY

2005-2006 Sabbathial leave from TUT; Position: Chief Scientific Officer, Bioretec, Ltd.

1995-2005 Tampere University of Technology, (**TUT**)
Academy Professor, Head of Institute

Research, development and consulting to the pharmaceutical and medical device industries in processing, structure, properties and medical applications of bioabsorbable synthetic polymers and composites. These materials are used to manufacture bioabsorbable surgical implants for orthopaedics and traumatology, maxillofacial surgery, plastic surgery, thoracic surgery and urology. Bioabsorbable implants are digested by living tissue, so they do not need a removal operation after tissue healing.

1996-2003 Bionx Implants Inc.,
Executive Vice President R&D, Board Member

Science and technology of synthetic bioabsorbable polymeric materials and ceramic materials, development of bioabsorbable implants for surgical applications

Accomplishments:

*Participated in founding Bionx Implants, Inc. with the mission of commercializing the self-reinforced, bioabsorbable polymer technologies developed in TUT. The company was sold in 2003 to Conmed Corp. and continues with the name Linvatec Biomaterials R&D and manufacturing at Tampere.

1986-1991 **TUT**
Research Professor of Academy of Finland, Institute Chairman

Research and development in polymer science and technology and in biomaterials.

1985-2005 **TUT**
Professor, Institute Chairman

Research, development, education and industrial consulting in polymer science and technology and in biomaterials.

Supervised inventor group, which managed as first in the world to develop ultra-high strength self-reinforced bioabsorbable polymeric composite materials for medical applications.

1984-1992 **Bionx Implants Ltd.**
Chairman

1983-1985 **TUT**
Professor of Textile Technology , Institute Chairman

Research, development, education and industrial consulting in fiber science and technology.

1975-1983 **TUT**
Associate Professor of Non-metallic Materials

Research, development, education and industrial consulting in science and technology of polymeric and ceramic materials.

AWARDS AND HONOURS

Inventor Award of Ministry of Trade and Industry 1987
Finnish Engineering Work Award 1988
Technology Award of Nordic Council 1988
Award of Tampere University of Technology 1993
Innovation Award (the third prize) of the President of Finland 1997
Award of Technical Creativity of Tampere City 1998
Reward of Foundation of New Technology (Turku, Finland) 1999
M.D. h.c. of University of Helsinki 2000
Technology Award of Technological Foundation 2005.

PATENTS

Main inventor or co-inventor in more than 200 international patents describing processing, structures, properties and medical or technical applications of synthetic polymeric, ceramic or composite materials.

PUBLICATIONS

More than 1000 international referee publications and printed conference abstracts of polymer science and technology, especially describing biopolymers and the medical applications.

BIOABSORBABLE OSTEOSYNTHESIS IN THE HAND: BIOMECHANICAL ANALYSIS

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INTRODUCTION

In unstable fractures and those associated with a complex hand injury, operative intervention and stable internal fixation of a bone are required. However, osteosynthesis devices become unnecessary or even harmful after consolidation. Bioabsorbable devices may offer clinical advantages in hand fracture fixation, but they must be of a composition and design to provide reliable and stable osteofixation. This study was undertaken to investigate the primary fixation stabilities provided by self-reinforced (SR) bioabsorbable hand bone fixation systems, in cases of transverse and oblique metacarpal osteotomies, using a cadaver human and pig metacarpal osteotomy models. These results were compared with those of standard metallic osteofixation.

MATERIALS & METHODS, RESULTS

Transverse metacarpal osteotomy (ref 1). One hundred twelve fresh-frozen metacarpals from humans had three-point bending and torsional loading after transverse osteotomy followed by fixation using seven methods: dorsal and dorsolateral 2-mm self-reinforced polylactide-polyglycolide (PLGA) 80/20 plating, dorsal and dorsolateral 2-mm SR poly-L/DL-lactide (PL(DL)LA) 70/30 plating, dorsal 1.7-mm titanium plating, dorsal 2.3-mm titanium plating, and crossed 1.25-mm Kirschner wires. In apex dorsal and palmar bending, dorsal SR-PLGA and P(L/DL)LA plates provided stability comparable with dorsal titanium 1.7-mm plating. When the bioabsorbable plates were applied dorsolaterally, apex palmar rigidity was increased and apex dorsal rigidity was decreased. Bioabsorbable platings resulted in higher torsional rigidity than 1.7-mm titanium plating and in failure torque comparable with 2.3-mm titanium plating.

In the oblique osteotomy study (ref 2), 160 fresh second metacarpal bones of domestic pigs were osteotomized and then fixed using bioabsorbable pins, screws or a plate. 1.5 mm SR poly-L-lactide (PLLA) pins provided fixation rigidity comparable with 1.5 mm Kirschner wires in dorsal and palmar apex bending, whereas in lateral apex bending and in torsion the rigidity was equal to that of 1.25 mm Kirschner wires. 2.0 mm SR-P(L/DL)LA 70/30 screws provided rigidity comparable with that of 1.5 mm Kirschner wires in all testing modes. The bioabsorbable plate considerably enhanced the bending stabilities of the fixation system, but a single interfragmentary screw provided only limited rotational rigidity.

DISCUSSION

The biomechanical results demonstrate that using SR implants, adequate fixation stability for hand fracture fixation can be achieved. We are in the early stages of treating fractures of the hand with SR-P(L/DL)LA 70/30 miniplates and screws. In preliminary three patients, with complex hand injuries, the SR-P(L/DL)LA 70/30 miniplates combined with 1.5 mm or 2.0 mm screws gave adequate stability for bone fixation and allowed union. The final conclusions await a larger series of fractures and long-term follow-up.

ACKNOWLEDGEMENTS

Financial support from the Finnish Academy, the National Technology Agency, the European Commission, and the Ministry of Education are acknowledged.

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- [3] Waris E et al (2004). *J Hand Surg* **29A**:452-457.
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Specialising physician in Surgery

Peijas Hospital, Vantaa

Master's degree:

2001 Kuopio, Finland

Doctorate:

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Relevant other experience relating to the application:

Assistant of Anatomy, Institute of Biomedicine/ Anatomy, Helsinki University, 12 mo during the years 1998-2001, Visiting Fellow, Institute for Craniofacial and Reconstructive Surgery, Province Hospital, Southfield Michigan, USA, Dr. Ian T. Jackson, 2 mo 1999; PhD student, National Graduate School of Clinical Investigation, January 2003 –

Representative publications:

1. **Konttinen YT, Kemppinen P, Li TF, Waris E, Pihlajamäki H, Sorsa T, Takagi M, Santavirta S, Schultz GS, Humphreys-Beher MG.** Transforming and epidermal growth factors in degenerated intervertebral discs. *J Bone Joint Surg* 81B(6):1058-63, 1999
2. **Xu J-W, Ma J, Li TF, Waris E, Alberty A, Santavirta S, Konttinen YT.** Expression of epidermal growth factor and transforming growth factor alpha in interfacial membranes retrieved at revision total hip arthroplasty. *Ann Rheum Dis* 59(10):822-827, 2000.
3. **Ceponis A, Waris E, Mönkkönen J, Laasonen L, Hyttinen M, Solovieva SA, Hanemaaijer R, Bitsch A, Konttinen YT.** Low-dose, non-cytotoxic, intra-articular liposomal clodronate delays development of erosions and prevents proteoglycan loss in established antigen-induced arthritis (AIA) in rabbits. *Arthritis Rheum* 44(8): 1908-16, 2001.
4. **Konttinen YT, Xu JW, Waris E, Li TF, Gomez-Barrena E, Nordsletten L, Santavirta S.** Interleukin-6 in aseptic loosening total hip replacement prostheses. *Clin Exp Rheumatol* 20, 485-490, 2002
5. **Wei H, Jyväsjärvi E, Niissalo S, Hukkanen M, Waris E, Konttinen YT, Pertovaara A.** The influence of chemical sympathectomy on pain responsivity and K adrenergic antinociception in neuropathic animals. *Neuroscience* 114(3) 655-668, 2002.
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7. **Waris E, Ashammakhi N, Happonen H, Raatikainen T, Kaarela O, Törmälä P, Santavirta S, Konttinen YT.** Bioabsorbable miniplating versus metallic fixation for metacarpal fractures. *Clin Orthop* 410:310-319, 2003.
8. **Waris E, Pakkanen M, Lassila K, Törmälä P, Konttinen YT, Suuronen R, Ashammakhi N.** Alloplastic injectable biomaterials for soft tissue augmentation: report on two cases with complications associated with a new material (DermaLive®) and a review of the literature. *Eur J Plast Surg* 26:350-355, 2003.
9. **Waris E, Ninkovic M, Harpf C, Ninkovic M, Ashammakhi N.** Self-reinforced bioabsorbable miniplates for skeletal fixation in complex hand injury. Three case reports. *J Hand Surg* 29A:452-457, 2004.
10. **Waris E, Ashammakhi N, Kelly C, Andrus L, Waris T, Jackson IT.** Transphyseal bioabsorbable screws cause temporary growth retardation in rabbit femur. *J Pediatr Orthop* 25(3):342-345, 2005